Do different time intervals in placement of restorative materials over calcium silicate cements, affect interface microhardness of different restorative materials?

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Abstract

Objectives: The type of materials and application time of final restorations on calcium silicate cements (CSCs) are important factors which influence the interfacial properties. The aim of this study was to investigate the effect of different placement time of RMGI (Resin Modified Glass Ionomer), composite resin and amalgam over different CSCs on the surface microhardness of these restorative materials.

Methods: Each CSCs material (Biodentine, MTA, CEM cement) was mixed and carried into a hole (6mm diameter ×4 mm thickness) in the center of 270 molds (n=90 /each CSC). Then these molds were randomly divided into three main experimental groups (n=30) in regard of restorative materials (Amalgam, RMGI, Composite) that were placed in the other molds with the same hole size to make restorative materials and CSCs in contact together. Afterwards, each experimental group was divided into three subgroups according to the time interval of restoration placement that was immediately, after 24h and after 72h (n=10). Two molds were separated from each other after one week storage in incubator with 100% humidity in 37 °C. in order to evaluate the Vickers microhardness of restorative materials in CSC-restorative material interface. Statistical analysis included two-way ANOVA followed by Post hoc Dunnett T3 in cases with lack of homogeneity and Tukey HSD in cases with homogeneity. (p<0.05)

Results: The microhardness of all restorative materials was neither significantly influenced by the CSCs materials (p>0.05) nor by the timing of final restoration (p>0.05) except in RMGI in immediate contact with CEM cement. (p<0.001)

Conclusion: Restorative materials hardness in interface with studied CSCs may not affect. This in vitro study found no evidence against immediate definitive restoration over CSCs.

Keywords: Calcium silicate cement; restorative materials; microhardness; time intervals.

Citation: Bolhari B, et al. (2021) Do different time intervals in placement of restorative materials over calcium silicate cements, affect interface microhardness of different restorative materials? Dentistry 3000. 1:a001
Received: March, 6, 2021
Accepted: April, 27, 2021
Published: September, 10, 2021
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Introduction

In recent years, application of biomaterials in dentistry, has resulted in improvement of various restorative and endodontic procedures [1]. Tooth preservation is an ultimate goal in modern dentistry. In this regard, vital pulp therapy (VPT) has gained considerable attention. The aim of VPT is keeping the dental pulp, vital and healthy following carious exposure or traumatic injuries. Some biomaterials can be used as a pulp protective layer in this procedure [2]. Ideally, these materials should be bioactive and biocompatible. Low solubility, ability to bind to dental tissues, adequate setting time and antibacterial activity are some of their characteristics too [3]. CSCs are bioactive materials which are used in many dental treatments like vital pulp therapy, repair of perforations and regenerative treatment. Nevertheless they have many favorable properties, difficult handling and tooth discoloration are considered as their disadvantages [4]. Mineral trioxide aggregate (MTA) was the first CSC introduced in endodontics [5]. Biodentine and Calcium-enriched mixture (CEM) Cement are known as CSCs that are fast setting dentine replacement material and claim to have no discoloration potential respectively [6]. Direct contact of cements with the final restoration happens in most clinical situations. The time span between the CSCs placement and final restoration could have an important role in success rate of treatments [7]. However, it is better to place final coronal restoration immediately after pulp capping to promote coronal seal and less microleakage, this is not possible because of long setting time in some CSCs for example MTA [8]. Resin-based composite, glass-ionomer cement (GIC), resin-modified GI (RMGI) and amalgam are common materials that are used for coronal restorations. The effect of immediate coronal restoration on the physical properties of different CSCs has been evaluated in few studies [9, 10, 11] but based on the authors’ search, it is assumed that the effect of the time of coronal restoration on the surface microhardness of restoration has not been assessed. Therefore, the aim of the present study was to investigate the effect of different time placement of RMGI, composite resin and amalgam over different CSCs on the surface microhardness of these restorative materials. It was hypothesized that the microhardness of restorative materials would not be affected by placement time.

Material and Methods

The materials used in the current study, manufacturer details, their composition and mode of application are shown in Table 1.

<table>
<thead>
<tr>
<th>Material</th>
<th>Manufacture</th>
<th>Composition</th>
<th>Mode of Application</th>
</tr>
</thead>
</table>
| Biodentine | Septodont, Saint Maur-des-Fosses, France         | Powder: Tri-calcium silicate, Di-calcium silicate, Calcium carbonate and oxide, Iron oxide, zirconium oxide  
Liquid: Calcium chloride, Hydro soluble polymer | One dose of liquid and powder mixed for 30 sec at 4000 rpm in an amalgamator      |

Table 1 – Materials composition and mode of application:
## Microhardness test:

In this in vitro experimental study, 540 cylindrical polymethylmethacrylate molds with a central hole with an internal diameter of 6 mm and height of 4 mm (according to ASTM E384 Standard for microhardness tests) were fabricated by CNC laser cutting (LaserProl, GCC, New Taipei City, Taiwan). Half of the molds were considered for CSCs which were placed on slabs and according to the CSC materials randomly divided into three main experimental groups (n=90). CSC material was prepared according to the manufactures instructions and placed in the molds. Then the rest of the molds were placed on each mold filled with CSC in a way that the two internal holes were positioned along each other. The second mold was used for restorative material placement. Afterwards, each main experimental group was divided into three subgroups (n=30) according to the restorative material applied. The time interval of restoration placement was varied. The final restoration was

<table>
<thead>
<tr>
<th>Material</th>
<th>Supplier</th>
<th>Powder Composition</th>
<th>Liquid Type</th>
<th>Preparation Method</th>
</tr>
</thead>
<tbody>
<tr>
<td>CEM Cement</td>
<td>BioniqueDent, Tehran, Iran</td>
<td>Powder: Calcium oxide, sulfur trioxide, phosphorous Pentoxide, silicon dioxide, aluminum trioxide, sodium oxide, magnesium oxide, chloride</td>
<td>Liquid: Water-based liquid</td>
<td>Mix Powder/Liquid ratio: 3/1</td>
</tr>
<tr>
<td>ProRoot MTA</td>
<td>Dentsply Maillefer, Ballaigues, Switzerland</td>
<td>Powder: Calcium carbonate, silicon dioxide, aluminum oxide, calcium zirconia complex</td>
<td>Liquid: Distilled Water</td>
<td>Mix powder/liquid ratio: 3/1</td>
</tr>
<tr>
<td>AdperTM Single Bond 2</td>
<td>3M ESPE, QuadrantLC, Cavex, Haarlem, Netherlands</td>
<td>BISGMA, HEMA, dimethacrylates, a methacrylate functional copolymer of polyacrylic and polyitaconic acids, ethanol, water, silica fillers, Camphorquinone</td>
<td>1. Apply 37% phosphoric acid etchant for 15 sec 2. Rinse for 10 sec 3. Apply 2 or 3 onsecutive coats of adhesive 4. Allow gentle air stream for 5 seconds 5. Light cure for 10 sec</td>
<td>1. Apply 37% phosphoric acid etchant for 15 sec 2. Rinse for 10 sec 3. Apply 2 or 3 onsecutive coats of adhesive 4. Allow gentle air stream for 5 seconds 5. Light cure for 10 sec</td>
</tr>
<tr>
<td>Amalgam</td>
<td>SDI, Victoria, Australia</td>
<td>Amalgam alloy and mercury</td>
<td>In amalgamator</td>
<td>In amalgamator</td>
</tr>
<tr>
<td>Filtek Z250 Composite resin</td>
<td>3M ESPE; QuadrantLC, Cavex, Haarlem, Netherlands</td>
<td>Filler: Zr/Si (60 vol%) 0.01-3.5µm Resin: BisGMA, UDMA, BisEMA</td>
<td>Light cure for 40 s</td>
<td>Light cure for 40 s</td>
</tr>
<tr>
<td>Fuji II LC Light cure glass ionomer</td>
<td>GC, Tokyo, Japan</td>
<td>Powder: Fluoro-alumino-silicate glass Liquid: poly-acrylic acid, HEMA, dimethacrylate, camphorquinone, water</td>
<td>Light cure for 40s</td>
<td>Light cure for 40s</td>
</tr>
</tbody>
</table>
Restoration microhardness in contact with CSCs


placed a. immediately b. after 24h and c. after 72h (n=10). There was no pretreatment prior to amalgam or glass ionomer placement but before placing composite resin in molds, total etch and bond (AdperTM Single Bond 2) preceded by etching with 37% phosphoric acid for 15 seconds was applied. Light curing time for both RMGI and composite resin was 40 seconds at 800 mW/cm² using a light-emitting diode (Woodipecker, china) light source.

Two molds were separated from each other after one week storage in incubator with 100% humidity in 37 °C, in order to evaluate the microhardness of restorative materials in CSC and restorative material interface. The side of restorative materials in contact with CSCs were polished using silicon carbide sandpaper with varying particle sizes of 400, 500, 800, 1000, 1200, 1500 and 2000 grit respectively. All the procedures were done by one person. For the purpose of facilitating indentation and minimizing the influence of sample preparation on surface microhardness, wet polishing with minimal hand pressure was employed. The surface microhardness test was performed using a Vickers Tester (Bareiss Prufgeratebau GmbH, Oberdischingen, Germany) and a pyramid shaped diamond indenter with a load of 300 g for 10 s. According to the pilot study this load created a clear and reliable indent in all three materials. Five indents were made on the polished surface of each sample at separate locations with a 2.5xd (2.5 times the mean diameter of each indent) distance between indentations and each indent from the edge of the sample (in accordance to ASTM E384 standard for Vickers microhardness test). The Vickers microhardness value (HV) was calculated by the testing machine based on the following equation:

\[ HV = \frac{2F \sin 136.7^\circ}{d^2} \]

\[ HV = 1.854 \frac{F}{d^2} \]

F= Load in kgf
d = mean of the two diagonals, d1 and d2 in mm
HV= Vickers microhardness value

Statistical Analysis

Statistical analysis included two-way ANOVA followed by Post hoc Dunnett T3 in cases with lack of homogeneity and Tukey HSD in cases with homogeneity.

Results

Mean and standard deviation of Vickers microhardness of different restorative materials in interface with verities of CSCs after several intervals, are listed in table 2.

Amalgam hardness in contact with all of CSCs increased insignificantly (P value = 0.32, 0.38 and 0.25 in contact with Biodentin, CEM cement and MTA respectively) over time. Hardness of composite in interface with different CSCs had no significant changes in different times (P value = 0.11, 0.25 and 0.21 in contact with Biodentin, CEM cement and MTA respectively). RMGI showed significantly decrease in hardness in contact with all of CSCs over time (P value = 0.001).

Comparison between restorative materials represented that hardness of RMGI is the least among them and amalgam had highest level of hardness contacting with all of CSCs. There was just one exception, RMGI had greatest hardness in contact with Cem cement immediately.
Table 2 – Mean±SD of the microhardness of different restorative materials in contact with CSCs in different times:

<table>
<thead>
<tr>
<th>Restorative Materials</th>
<th>Biodentin</th>
<th>Cem cement</th>
<th>MTA</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Immediate</td>
<td>24h</td>
<td>72h</td>
</tr>
<tr>
<td>Amalgam</td>
<td>186.60±9.09 a</td>
<td>188.86±17.79 a</td>
<td>199/00±28.63 a</td>
</tr>
<tr>
<td>Composite</td>
<td>136.20±9.77 b</td>
<td>116.13±13.75 b</td>
<td>122.90±3.01 b</td>
</tr>
<tr>
<td>RMGI</td>
<td>125.90±6.66 c</td>
<td>97.37±5.26 d</td>
<td>99.00±28.63 d</td>
</tr>
</tbody>
</table>

*Different letters show significant differences between groups

Discussion

There are some kinds of materials known as calcium silicate cements (CSCs) that recommended for pulp capping process. They provide pulp vitality maintenance and stimulate making growth factors and lead to dentin formation in asymptomatic teeth [12]. Some characteristics are considered for these pulp capping materials like biocompatibility; dimensional stability; insolubility in tissue fluids; easy manipulation; adhesion to the tooth structure; providing adequate seal and remaining in place under dislocating forces [13]. Among different factors affected pulp therapy prognosis, the time of the placement of well-sealed permanent coronal restoration is critical. Glass-ionomer cement (GIC), resin-modified GI (RMGI) Resin-based composite, and amalgam are common materials for coronal restorations [14]. When restorative materials are applied on CSCs immediately or after different intervals, it may that setting reactions of each materials affect the other one setting in the interface between them. Timing of coronal restoration placement on the physical properties of CSCs has been evaluated in some studies [14, 15, 16] but there is no study about the effect of the coronal restoration placement time on the surface microhardness of restorative materials. Therefore, the aim of the present study was to investigate the microhardness of RMGI, resin composite and amalgam restoration in interface with different CSCs after different time intervals. Hardness is a property of major importance for assessing the adequate setting of restorative materials [17] It not only represents deformation resistance but also shows stability of material crystalline structure. As there is an inverse relationship between hardness and porosity, adequate levels of hardness play an important role in achieving an ideal seal [18]. Hardness is one of the determinants of the life time of dental materials and prevent restorative material displacement.
and disruption of the physical seal during masticatory occlusal loads [19].

As it is possible to perceive, amalgam hardness in contact with three CSCs used in this study, had an acceptable measure that increased insignificantly with time. This finding showed that amalgam hardness in interface was not affected by the CSCs' hydration process even when immediately placed.

Increasing amalgam hardness over time could be attributed to continuous crystallization of amalgam over time because of the setting reaction rate which is somehow slow and takes several days to be completed [20]. So, it seems that setting conditions of CSCs have no adverse effect on amalgam strength [17]. In contrast some factors like the pH value of the environment, the condensation pressure, humidity and temperature may affect microhardness of CSCs that it has been studied in many researches [21].

In this study composite reached to optimum microhardness in interface and no adverse effect were seen in composite setting reaction in contact with CSCs and no significant changes in hardness was seen in different placement times. Correlation between the microhardness and the degree of conversion of composite resins have shown in several studies [22] the results of the present study showed that the degree of cross linking in the polymerized matrix reaches the maximum hardness immediately after light curing and it does not change in contact with CSCs setting reaction in different intervals especially in immediate composite placement [23]. In case of immediate coronal restoration, clinical manipulations including the condensation pressure, etching, rinsing, and priming could affect the setting of CSCs [15]

RMGI showed significantly decrease in hardness in contact with all of CSCs over time. The reason may be because of moisture absorption from CSCs by RMGI until microhardness test was done so environment humidity result in water sorption in RMGI. Amalgam and composite are somehow stable materials in presence of humidity, where their water sorption and degradation rate is very low compared with RMGI that present higher degradation and lower hardness values [12]. In a study by Ambrosano it was shown that after RMGI degradation in moisture conditions, the hardness decreased significantly in this material [24]. Comparison between restorative materials represented that hardness of RMGI is the least among them and amalgam had maximum hardness contacting with all CSCs and in all time intervals. This is not unexpected results because of materials mechanical properties as shown in literature that amalgam, composite and RMGI have the highest measure of hardness respectively [25]. There was just one exception in the present study, RMGI had the greatest hardness in contact with Cem cement immediately. In studies by Cantekin and Doozaneh was shown that Cem cement consist of different calcium compounds that can bond chemically with RMGI especially when placed immediately over CEM cement that have not been fully set [26,27]. it is supposed during separation of two molds, because of chemical bonding, pieces of CEM cement would remain on the RMGI surface and the higher amount of microhardness was associated with that.

This was an in vitro study; therefore, the condition of the oral cavity wouldn’t completely have simulated. In this study just microhardness was evaluated, therefore, it is suggested that other characteristics like microleakage and bond strength between
different types of restorations and several CSCs, would be studied [28]. It should be noted that in another study, done by the authors, the microhardness of CSCs is evaluated and the results of these both studies will be useful in determination of placement time of restorative materials over CSCs [29].

**Conclusion**

Within the limitation of this laboratory study, it was concluded that there is no difference between placement time of restorative materials over studied CSCs in regards of the restorative material microhardness. So immediate placement of a final restoration over CSCs not only provide better coronal seal but also would be clinically beneficial for patients and dentists, decreasing time and cost.

**Conflicts of interest**

The authors declare no competing interest.

**Availability of data and materials**

The data that support the findings of this research are available from the corresponding author [S.V] upon request.

**References**

10. Ha HT. The effect of the maturation time of calcium silicate-based cement (Biodentine™) on

